

BioTechMed-Graz

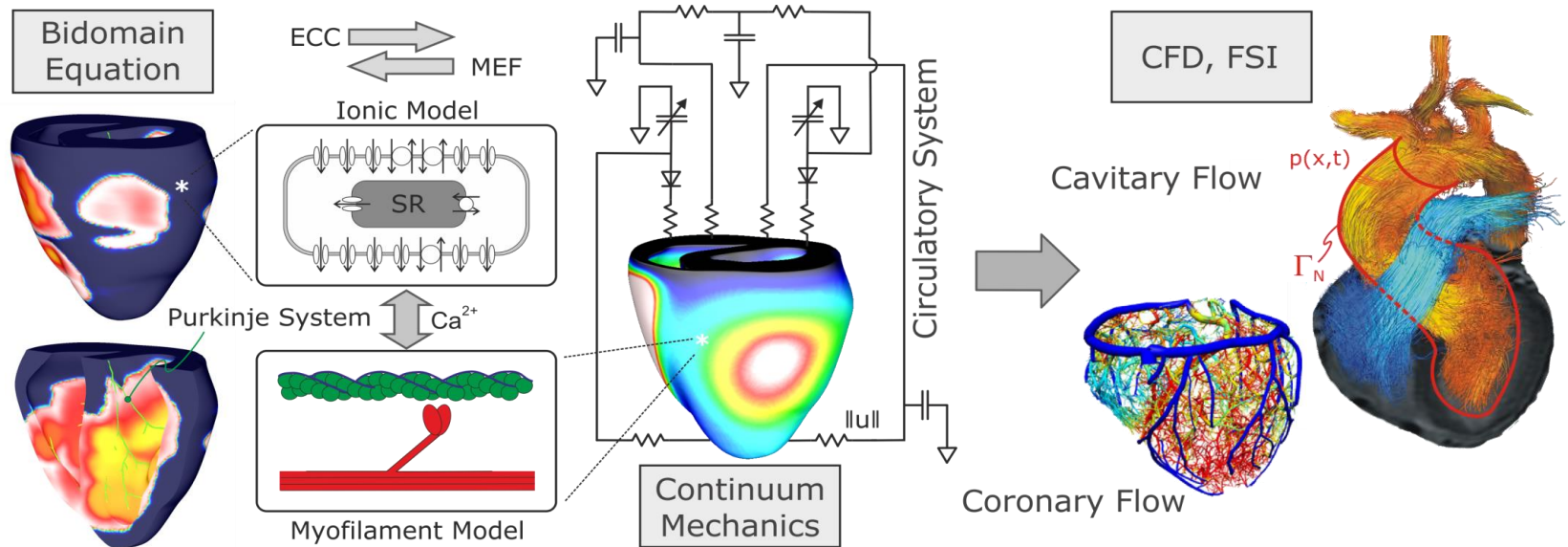


*Biomedical Basics-**T**echnological Developments-**M**edical Implementation*

Research for Health

Quantitative Biomedicine & Modelling

Computing a heart beat



- **Modeling and Computing**

- Electrophysiology (EP)
- Non-linear Elasticity
- Fluid Flow
- Porous Media Flow

- **EP Applications**

- Arrhythmogenesis & Defibrillation

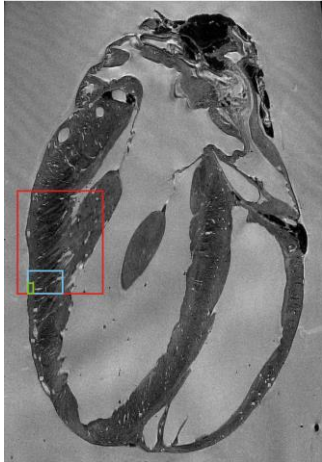
- **Mechanics Applications**

- Heart Failure and CRT

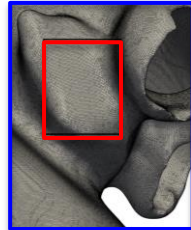
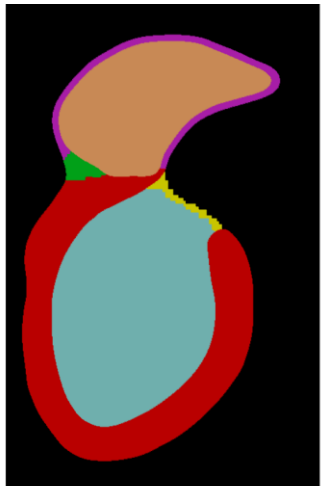
- **Flow Applications**

- Aortic Valve Disease and Coarctations

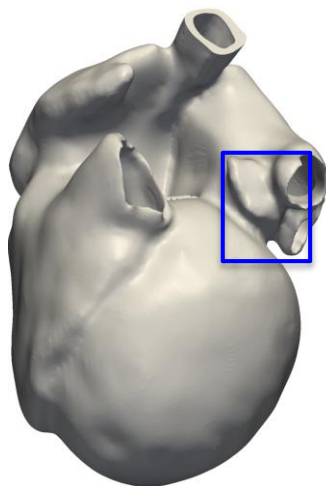
Imaging



Segmentation



FE Meshing



Mathematical Description

$$\nabla \cdot (\boldsymbol{\sigma}_i + \boldsymbol{\sigma}_e) \mathbf{C}^{-1} \nabla \phi_e = -\nabla \cdot \boldsymbol{\sigma}_i \mathbf{C}^{-1} \nabla V_m - I_e$$

$$\nabla \cdot \boldsymbol{\sigma}_i \mathbf{C}^{-1} \nabla V_m = -\nabla \cdot \boldsymbol{\sigma}_i \mathbf{C}^{-1} \nabla \phi_e + \beta I_m$$

$$I_m = C_m \frac{\partial V_m}{\partial t} + I_{\text{ion}}(V_m, \boldsymbol{\eta})$$

$$V_m = \Phi_i - \Phi_e$$

$$\frac{\partial \boldsymbol{\eta}}{\partial t} = f(\boldsymbol{\eta}, V_m, \sigma_a)$$

$$\text{div } \boldsymbol{\sigma}(\mathbf{u}) = \mathbf{b},$$

$$\boldsymbol{\sigma} = \boldsymbol{\sigma}_p + \boldsymbol{\sigma}_a$$

$$\boldsymbol{\sigma}_p = J^{-1/3} \bar{\mathbf{F}} \left(2 \frac{\partial \Psi}{\partial \mathbf{C}} \right) \bar{\mathbf{F}}^T$$

$$\boldsymbol{\sigma}_a = \sigma_a(\bar{\mathbf{f}} \otimes \bar{\mathbf{f}})$$

$$\sigma_a = h(V_m, \boldsymbol{\eta}, \lambda, \dot{\lambda})$$

ECC

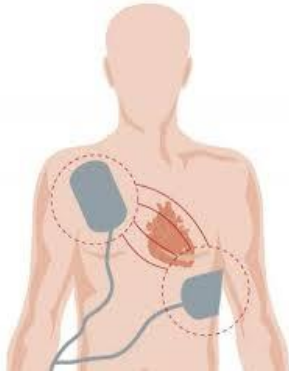
MEF

EP

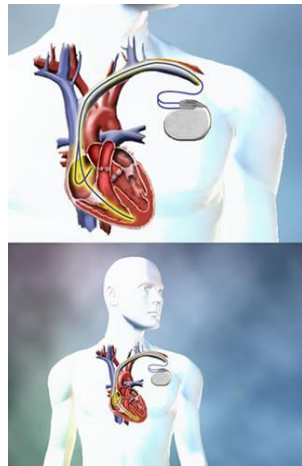
Deformation

EP and mechanics are bidirectionally coupled through excitation-contraction coupling (ECC) and mechano-electric feedback (MEF)

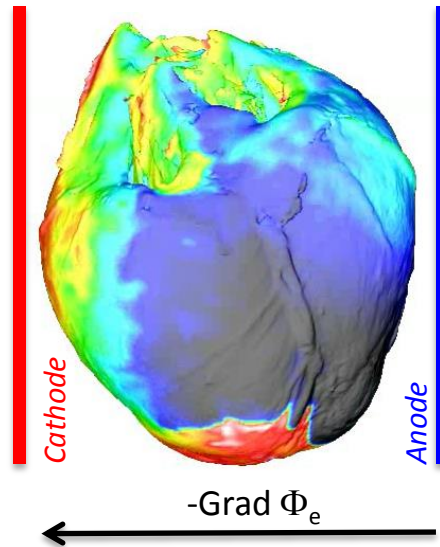
„External“



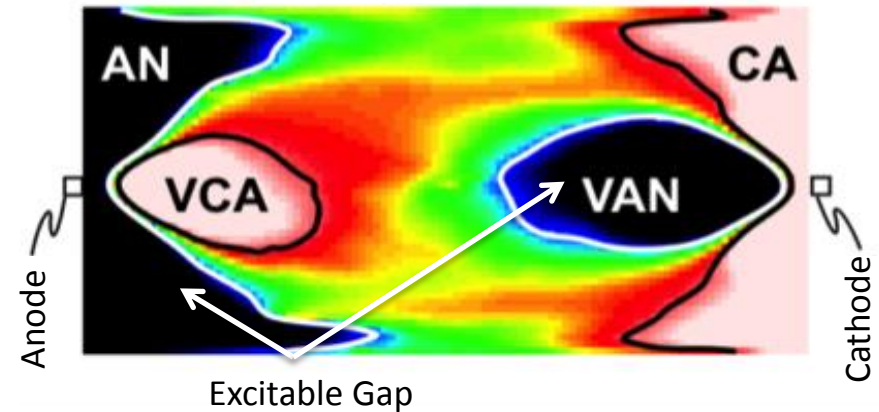
„Internal“



Shock Delivery

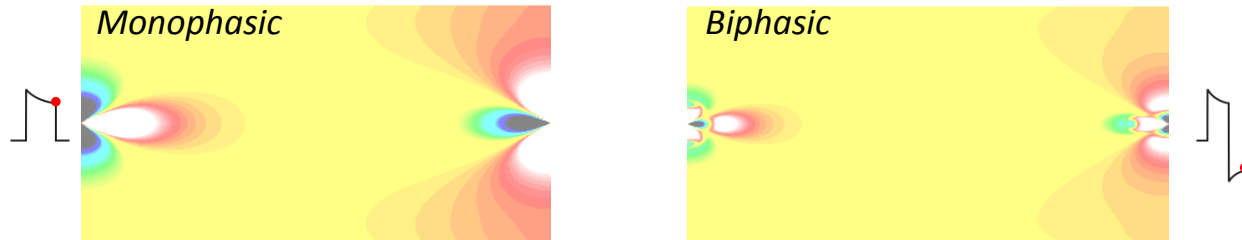


Postshock Virtual Electrode Polarization



- Only reliable therapy to prevent Sudd Cardiac Death
- Detrimental effects affect Quality of Life (Pain Perception)
- Stochastic phenomenom, success depends on strength, location, timing, polarity and pulse shape of shock

Tissue Response to Defibrillation Shock – Dependency on Shock Waveform

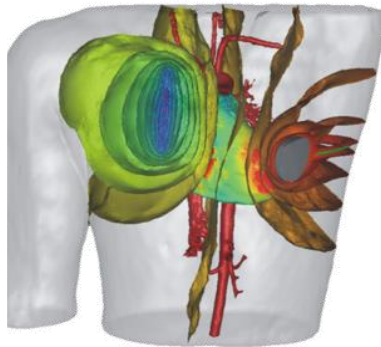


PDE Constrained Optimization

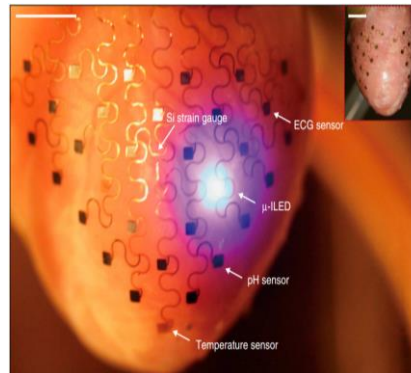
$$\mathcal{L}(V_m, w, I_e, p, q) = J(V_m, I_e) + \langle e(V_m, w, I_e), (p, q) \rangle$$

$$J(V_m, I_e) = \frac{1}{2} \int_0^T \left(\int_{\Omega_{obs}} |V_m - V_d|^2 d\Omega_{obs} + \alpha \int_{\Omega_{con}} |I_e|^2 d\Omega_{con} \right) dt$$

Optimize Lead Placement



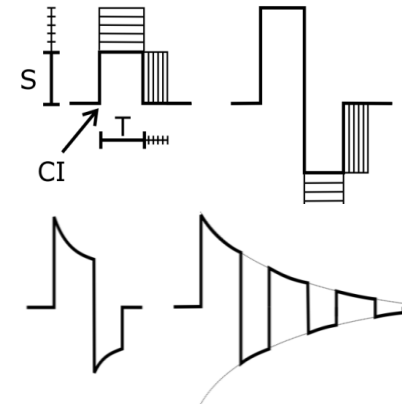
Subcutaneous ICD



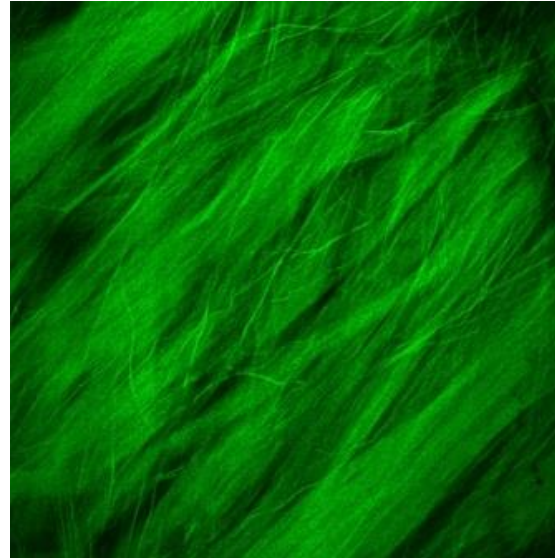
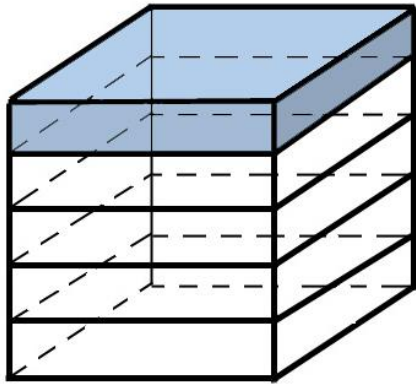
Wide Area Defibrillation

Xu et al, 5:3329, Nature Comm

Optimize Timing/Pulse Shape



- Image stack (z-stack)



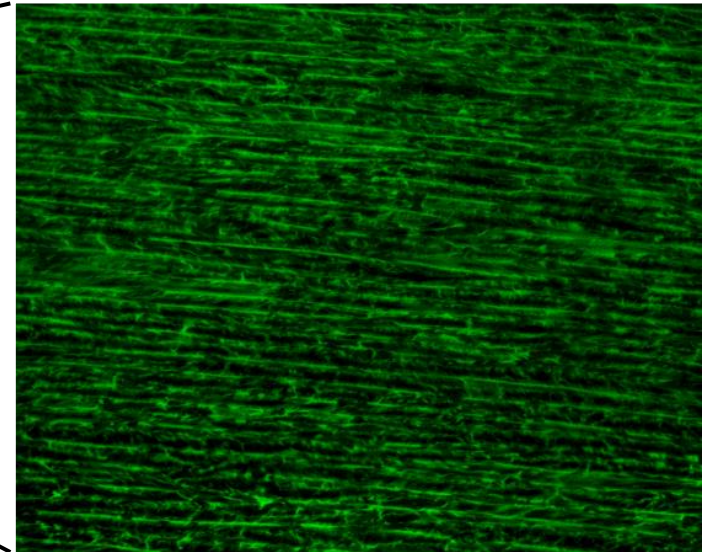
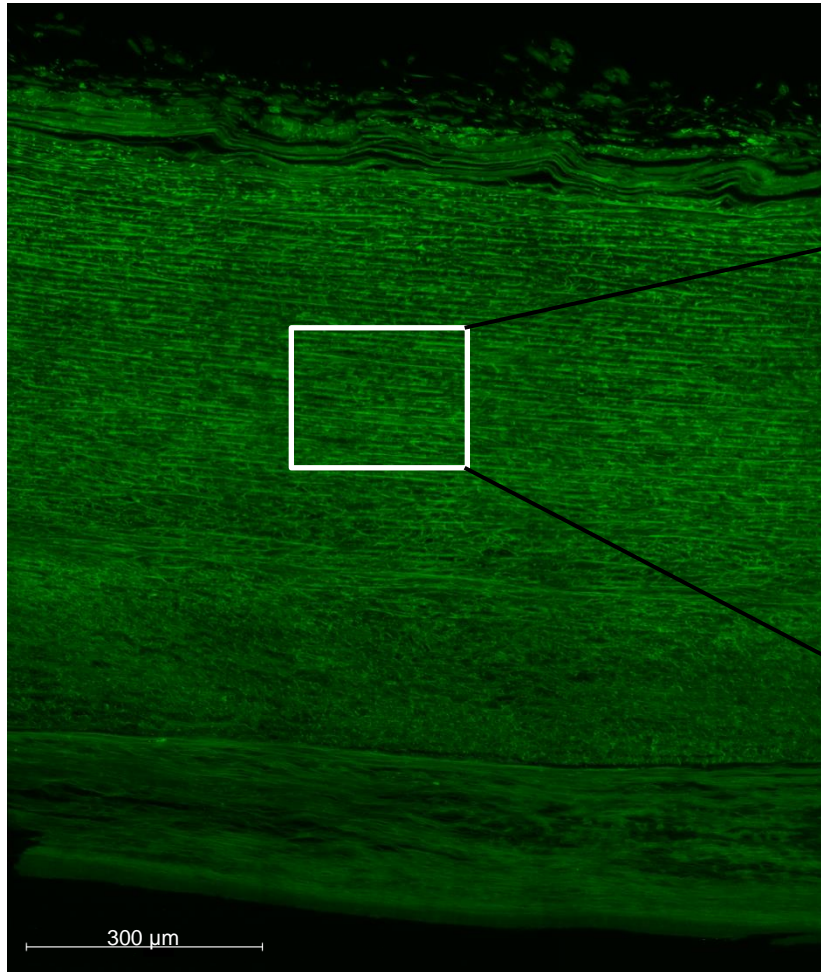
Collagen fibers in the human adventitia

- Image size (25x water objective)
 - 534 x 534 μm
- Image depth
 - 300nm
- Distance between images
 - 1 μm



Human abdominal aorta before and after optical clearing
Schriebl et al. [RSI], 2013

- In-plane collagen fibers in the human media



Cross section of a healthy arterial wall
 $p = 120 \text{ mmHg}$, axial pre-stretch: 12%

- **Material and structural modeling**

- Strain-energy function of the artery wall

$$\Psi_{\text{iso}} = \Psi_g(\bar{\mathbf{C}}) + \sum_{i=4,6} \Psi_{fi}(\bar{\mathbf{C}}, \mathbf{H}_i)$$

- Energy stored in the two families of dispersed collagen fibers

$$\Psi_{fi}(\bar{\mathbf{C}}, \mathbf{H}_i) = \frac{k_1}{2k_2} [\exp(k_2 \bar{E}_i^2) - 1], \quad i = 4, 6$$

- Green–Lagrange strain-like quantity

$$\bar{E}_i = A\bar{I}_1 + B\bar{I}_i + (1 - 3A - B)\bar{I}_n - 1$$

A and B consider the measured **structure** of the collagen fibers

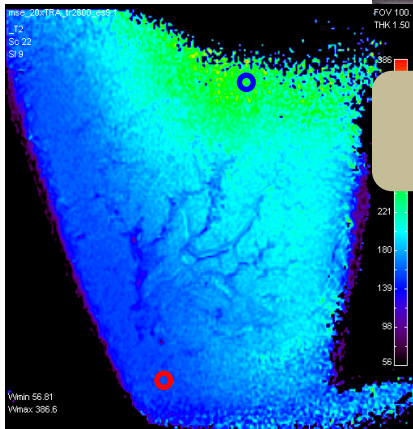
- The development of MRI towards a biomarker imaging technique by the application of advanced MR principles and mathematical methods. (SFB Mobis).

Speed



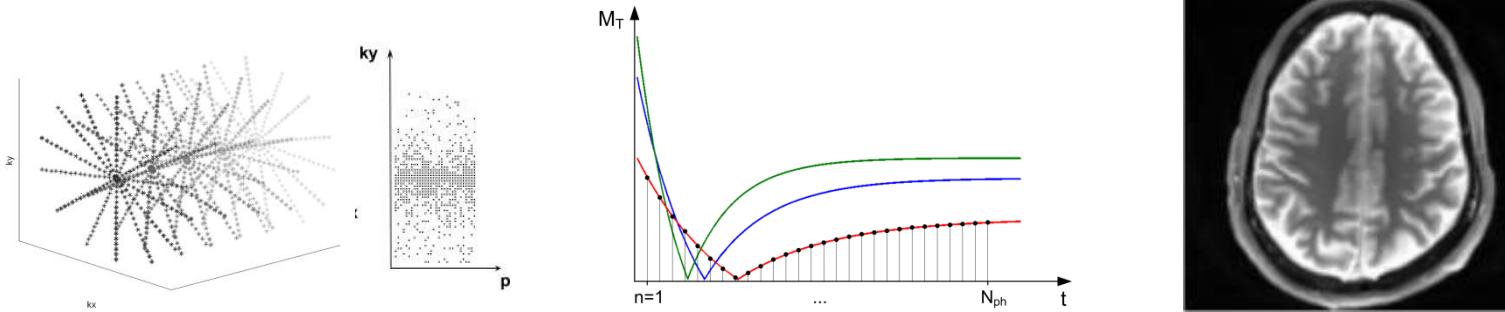
Integrated
quantitative
procedures

Robustness



$$F(z) = \frac{M_0}{2} \left(1 + \sqrt{\frac{(1 + zE_2)[1 - z(E_1 + E_2) \cos \alpha + z^2 E_1 E_2]}{(-1 + zE_2)[-1 + z(E_1 - E_2) \cos \alpha + z^2 E_1 E_2]}} \right)$$

Integrated Proc: Multiparameter MRI (mpMRI)



mpMRI:

1. Multiple parameter encoding

$$s_n(T) = \|\vec{M}_n(x, y)\|$$

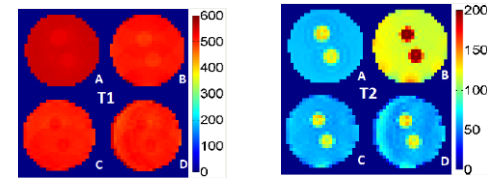
$$\vec{M}_n = \frac{1}{K} \sum_{k=1}^K \mathbf{E} \mathbf{R}_x(\alpha_{n,k}) \mathbf{R}_z(\pi) (\mathbf{E} \vec{M}_{n-1} + \vec{e}) + \vec{e}$$

2. Generating function for transient sequences

3. Model based reconstruction

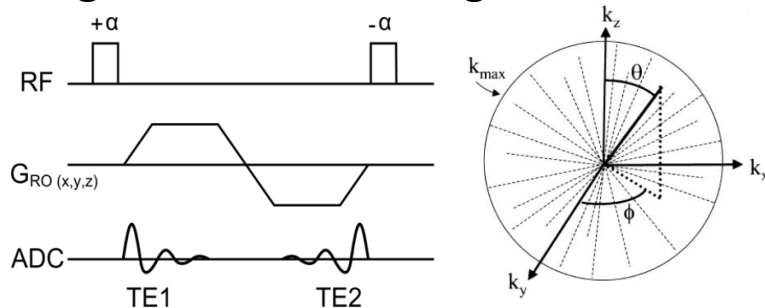
$$\min_{T=\{T_1, T_2, M_0\}} \frac{1}{2} \sum_{c,n} \|\mathcal{P}_n \mathcal{F}(c_s s_n(T)) - d_{n,c}\|_2^2 + \lambda \text{TGV}(T)$$

Visibility study
Phantom T1,T2

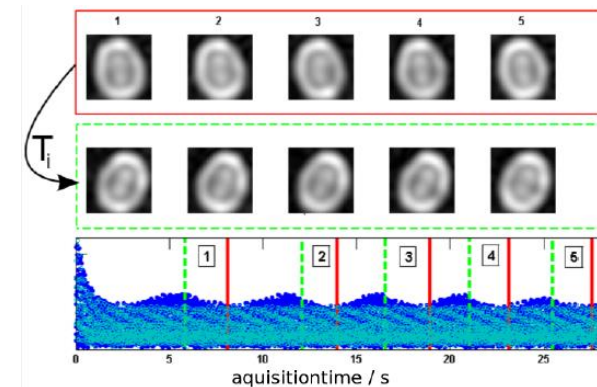


- Body motion is still a problem for MRI
- **Goal: retrospective motion correction**

e.g. 3D radial scanning



Low
resolution
Subsets
 \Rightarrow



Forward operator model with
mapping of motion dependent
position to k-space data

$$K : u \mapsto \sum_{t=1}^N \mathcal{F}_t(b_j T_t u)$$

Challenges and research objective:

- Motion correction of time-resolved 3D radial acquisitions for free-breathing dynamic MRI
- Motion correction high resolution 3D
- Investigation new math. Approaches



❖ 3T MRI (Research System)

Siemens Skyra, 45mT Gradient, different Array coils, Head Coils with 20 and 32 channels, Mouse & Rat coil., fMRI equipment, Elastography unit.

❖ Pulse programming capabilities

❖ Advanced signal modelling

❖ Fast offline reconstruction for new algorithms

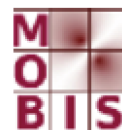


Inverse Problems & Mathematical Imaging

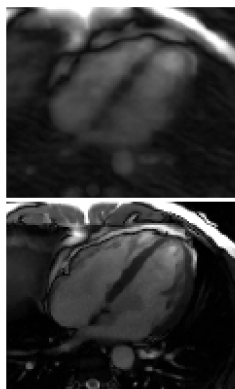
Institute for Mathematics and Scientific Computing

Fields of research

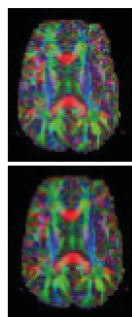
- Variational modelling and optimization for advanced reconstruction and quantification of image data
- Application to medical imaging (MRI/CT), microscopy, and beyond



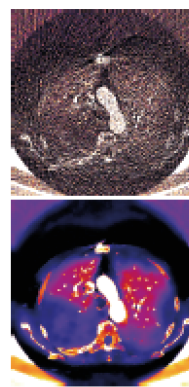
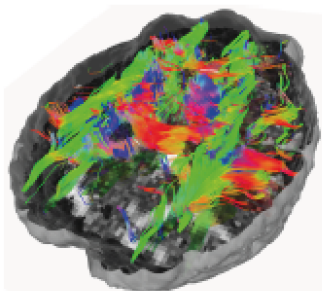
SFB Research Center
Mathematical Optimization &
Applications in
Biomedical Sciences



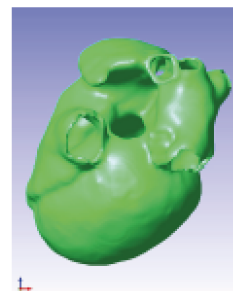
Dynamic MRI



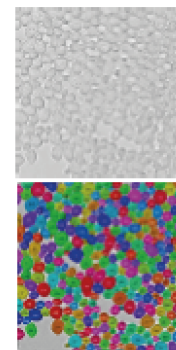
Regularized DTI



Dual-Energy CT



Binary surface
smoothing



Cell
segmentation

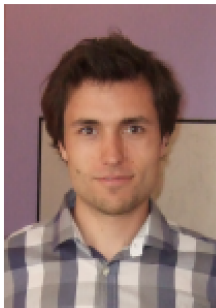
Inverse Problems & Mathematical Imaging



Univ.-Prof. Dr. Kristian Bredies

Head of group

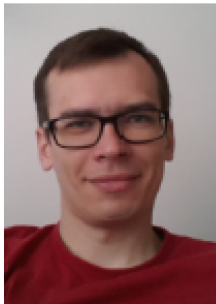
- Advanced imaging techniques/Inverse problems
- Optimization and variational approaches



Dr. Martin Holler

Postdoctoral researcher

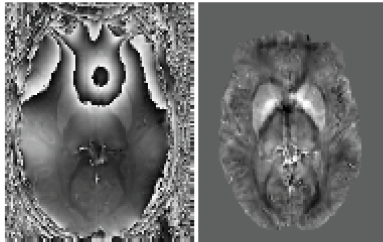
- Dynamic imaging and reconstruction
- Image/Video compression techniques



Dr. Kamil Kazimierski

Postdoctoral researcher

- Image data analysis and quantification
- Regularization approaches for inverse problems

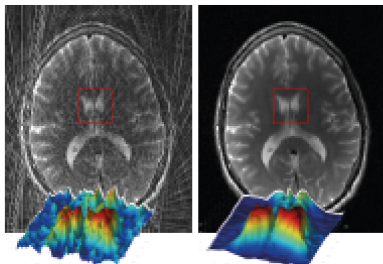


Inverse Problem: Quantitative susceptibility mapping

$$\text{TGV}_\alpha^2(u) = \min_{w \in \text{EBD}} \alpha_1 \|\nabla u - w\|_{\mathcal{M}} + \alpha_0 \|\mathcal{E}w\|_{\mathcal{M}}$$



Advanced regularization



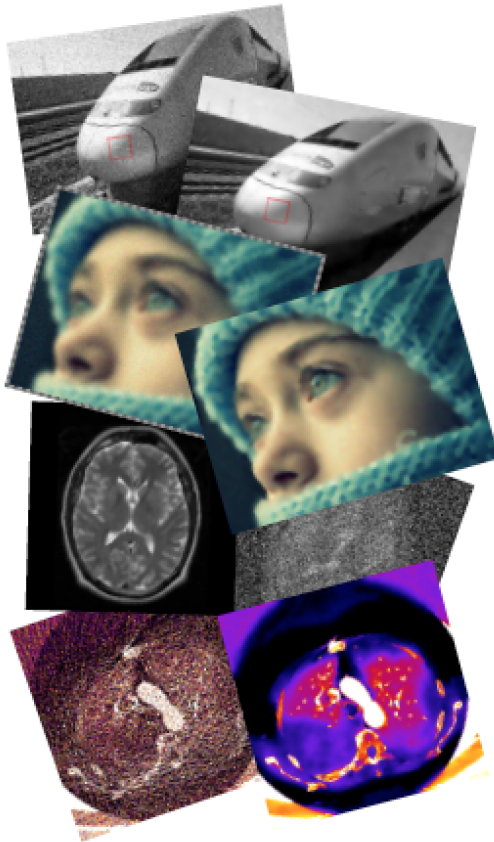
Compressed sensing in MRI
(10% of the data)

Inverse problems: How to reconstruct from measurements?

- Modelling: Describe measurements process
- Inversion: Find solution explaining given measurements
- Regularization: Make solution reasonable
- Optimization: Find best of out many solutions

Recent developments

- Inverse problem paradigm becomes established in medical imaging
- Development of advanced regularization approaches
- Compressed sensing: Reconstruction from few measurements
- Availability of powerful optimization algorithms



Available expertise

- Image enhancement:
Denoising, deblurring & beyond
- Modelling and realization of
reconstruction strategies
- Reconstruction from incomplete data
- 2D/3D image data & image sequences

BioTechMed Graz

- Strengthen cooperations with practitioners
- Improve mathematical models
- Enhance efficiency of numerical algorithms

BioTechMed[®]
GRAZ

